EUROPEAN COAL AND STEEL COMMUNITY

Community Ergonomics Research

Translations: French, German,

Italian

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Technical Report Nº 24

A METHODOLOGY FOR EVALUATING HIGH WORK LOADS

Source : Ergonomics Team of the U.K. Steel Industry

Authors: J.E. CRAWLEY, J. MUSGROVE, R.B. PLENTY

Reference period: 1.1.1974 - 31.8.1975

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CONTENTS

			Page
SECTI	ON I:	Summary Report	1
SECTI	ON II:	Technical Report	1
1.0	INTRODUC	CTION	1
2.0	METHODS		2
	2.1	Data Acquisition	2
	2.2	Heart Rate	2
	2.3	Environmental Data	4
	2.4	Activity Coding	6
	2.5	Energy Expenditure	6
	2.6	Electromyography	6
	2.7	Subjective Estimates of Fatigue	7
	2.8	Questionnaire	9
3.0	LABORATO	DRY SIMULATION OF MANUAL METAL ARC WELDING	9
4.0		R 12 MONTH PERIOD ENDING MARCH 1976 tion: 6245. 35/8/002)	9
	4.1	Laboratory Studies	9
	4.2	Field Work	12
5.0	APPENDIC	CES	12
	5.1	Appendix I - Crystal Timer Circuit Description	12
	5.2	Appendix II - Description of Activity Coding Device	14
	5•3	Appendix III - Heart Rate Data Collection and Analysis	19
	5.4	Appendix IV - Subjective Ratings of Fatigue	41
	5•5	Appendix V - Questionnaire and Fatigue Ratings for Works Based Measurements	42
6.0	REFERENC	CES	68
7.0	ACKNOWT.	CDGEMENTS	69

SECTION I

SUMMARY

This is the final report for Part I of this project and reports the methodology that has been developed for use in the three years of Part II. The methodology is largely centred around the use of miniature, four channel, analogue tape recorders with an analysis system that depends on a PDP 11/45 computer for analogue to digital conversion and an ICL 1904s for data analysis and presentation.

Some of the laboratory work outlined in the plan for the next twelve months has in fact been started during the development work of Part I. Continuing parallel studies of laboratory assessment of fatigue and works identification of stress situations have been planned.

SECTION II

1.0 INTRODUCTION

There were two main objectives for the first year of this study. The first was to establish reliable, non disruptive methods of collecting physiological and environmental data in steelworks. The second was to establish laboratory methods of assessing operator fatigue whilst performing simulated steelworks jobs.

The application of this methodology is in the identification of stress situations in the industry and detailed investigation of these stresses in the laboratory. The outcome of any such investigation will depend largely on the job being evaluated. (Wherever possible routines of work and rest periods will be investigated.) In many situations however the task dictates the work pattern and therefore work-rest regimes are impossible to implement. In these

1248/76 e - ACE

situations job rotation will be considered as a means of reducing stress.

In order to evaluate our methodology as it developed a simulated task was set up in the laboratory. The simulation consists of a device that reproduces the postures and movements made in manual metal arc welding. An initial series of experiments on the combined effect of welding and posture was begun during this part of the project.

2.0 METHODS

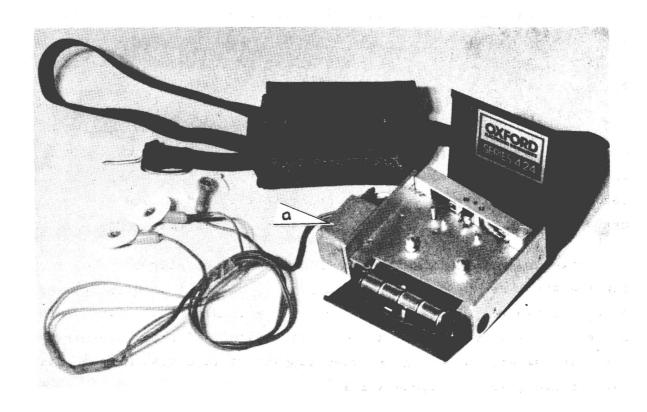
2.1 Data Acquisition

Data acquisition of all transducable parameters is accompliance by the use of small, four channel analogue tape recorders (plate 1). This MEDILOG (Oxford Instrument Co. Ltd.) recorder can record analogue information on three channels. The fourth channel carries a 1 Hz crystal controlled timing device designed by BSC engineers (Appendix 1). The accuracy of this device allows precise matching of data from different recorders. The recording speed is 2 mm/sec and replay speed 50 mm/sec. The output from the replay machine (plate 2) is fed simultaneously into an oscilloscope, a pen recorder and the analogue to digital converter of a PDP 11/45 computer.

Digitized data from the PDP 11/45 is stored on magnetic tape for later analysis on an ICL 1904s computer.

2.2 Heart Rate

Heart rate is recorded as the electrocardiogram (ECG) using the system described in 2.1. Three chest electrodes (Cambridge Instrument Co. Ltd.) of the stick on type are used. The output from the ECG replay amplifier is fed via a pulse interval timer (PIT)



<u>Plate 1</u> - A MEDILOG recorder with electrodes and carrying case a. Modified input socket

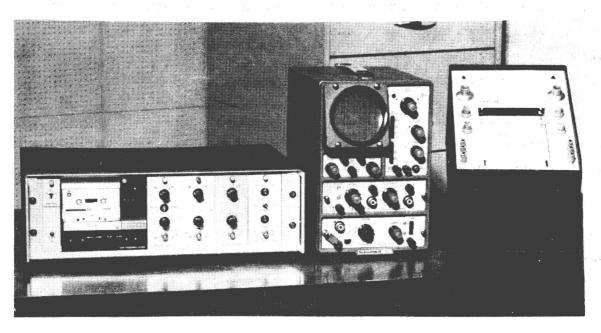


Plate 2 - The tape replay unit with replay amplifiers and puls interval timer. The oscilloscope and pen recorder are used for monitoring during replay onto the computer.

module in the replay unit (plate 2) to the computer. The PIT produces a 20 volt spike for each QRS complex. This spike (reduced to less than 5 volts) is counted, timed by the computer and, together with the 1 Hz timing pulse, stored on magnetic tape.

The stored heart rate information is processed by an ICL 1904s computer. The first stage calibrates the PIT pulses against the 1 Hz timing pulse and so produces a list of inter beat intervals (IBI). The second stage is a noise detection analysis that recognises extraordinarily long or short pulses and substitutes a mean value.

Inter beat interval analysis produces a graph plot of heart rate for the whole recording. The normal plot is of heart rate calculated every O.l minutes; however more, or less, accurate resolutions can be programmed. Maxima, minima and means for individual activities are given in summary tables. A detailed account of this system plus example outputs are given in Appendix III.

2.3 Environmental Data

Environmental measurements of temperature (wet bulb, dry bulb, globe) are monitored continuously. These measurements are recorded sequentially onto a single channel of the tape recorder in order to allow the other two channels (the fourth channel carries a timing pulse) to be used for such parameters as noise and air speed.

The measurement of environmental conditions is made using a light laboratories WBGT meter (plate 3) modified to give sequential output to the rape recorder automatically every 15 seconds.

Computer handling of temperature data gives graph plots of computed information such as mean radiant temperature and corrected effective temperature.

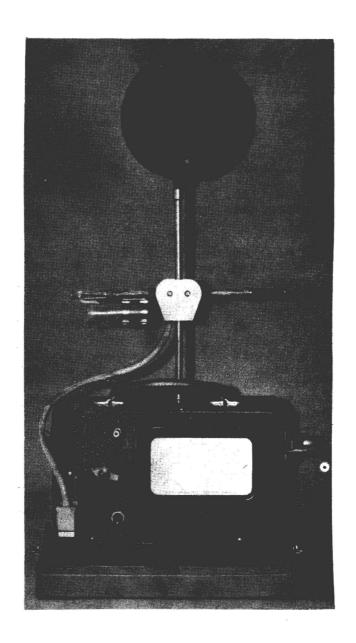


Plate 3 - Light laboratories WBGT meter

2.4 Activity Coding

Analysis of physiological and environmental data from either the works or laboratory simulation studies is only possible if this data can be related precisely to the activity of the operator or subject under study. In order to simplify the recording of activity information a sixteen channel keyboard operated device has been designed to record onto two channels of a miniature tape recorder. Each channel carries four levels of DC signal. A combination of any two of these signals allows 16 codes to be used. The third channel carries an interrupt signal every time the code changes and the fourth channel carries the timing pulse. The interrupt signal triggers the computer to read the new code during the analysis of this data. Analysis is by PDB 11/45 computer which thus provides the activity information for parallel processing with any other set of data i.e. heart rate or environmental conditions. Description of this activity coding device is given in Appendix II.

2.5 Energy Expenditure

In the laboratory a conventional Douglas Bag technique is used to measure oxygen consumption. Expired air is collected via a two way valve and mouthpiece into large plastic vinyl bags. Gas volume is measured using a Parkinson Cowan CD4 gas meter. Gas analysis is carried out using a Servomex portable oxygen analyser and a Horiba portable carbon dioxide analyser. Spot checks on gas analysis are made using a Lloyd-Haldane apparatus.

2.6 Electromyography

Localised muscle fatigue due to static work loads is difficult to quantify by conventional methods of either heart rate measurement or

energy expenditure. An attempt to quantify this kind of fatigue by changes in electromyographic (EMG) recordings is being made.

In particular these changes relate to the spectral qualities of the signal (Kadefors¹). Other changes associated with fatigue (Edwards and Lippold², Vredenbregt³) relate to the relative levels of electrical activity, and can also indicate fatigue. This type of result however must be treated with caution (Kadefors¹) due to the increase in these parameters as a result not only of fatigue but also of an increase in force of contraction.

Changes in spectral quantities of EMG shown by other workers (Chaffin⁴, Petersen⁵) will be investigated as a means of quantifying local muscle fatigue.

Surface electrodes are used of the silver disc type and placed longitudinally over the belly of the muscle 2 cm apart (\mathbb{Z} uniga 6).

Amplification of EMG signals is made using a six channel MEDELEC amplifier (plate 4). Recording is made onto a SANGAMO FM tape recorder. Subsequent frequency analysis of one second samples of EMG data is performed by a) Analogue to digital sampling (2000 times/sec) on a PDP 11/45 computer and b) Fast Fourier Transformation of this data on an ICL 1904s computer. The resultant analysis gives a power spectrum from 10-1000 Hz with a resolution of 1 Hz.

The computer output gives a 'decibel' against 'log of the frequency' plot of each 1 second sample plus root mean square, mean rectified average and amplitude or percentage power of any designated frequency band.

2.7 Subjective Estimates of Fatigue

In order to help locate anatomical areas of fatigue a general and local fatigue score is made. Details of the scoring technique and analysis procedures are given in Appendix IV.

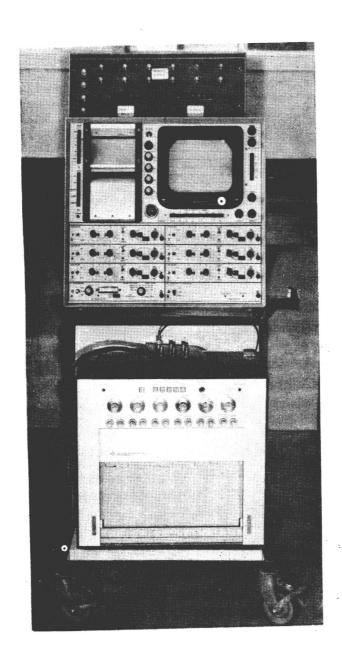


Plate 4 - MEDELEC EMG amplifiers and recorder.

The six channel pen recorder is used for monitoring during recording sessions.

2.8 Questionnaire

Any job evaluation and subsequent reorganisation must take into account the attitudes of operators engaged on the job as it already exists. To this end we have designed a questionnaire that we hope will encourage worker participation in job design. A detailed account of this questionnaire is given in Appendix V.

3.0 LABORATORY SIMULATION OF MANUAL METAL ARC WELDING

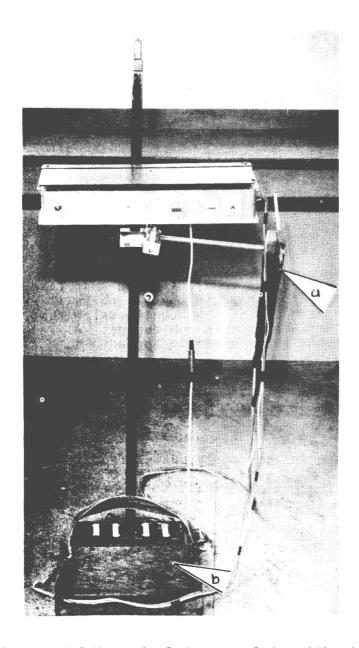
This equipment, described in the 1st technical report for this project, has been completed and is shown in plates 5 and 6. Plate 6 shows the drive motor, track and photoelectric cell carriage. The carriage is drawn along the track only when the photoelectric cell is energised by a small light on the tip of the 'electrode' (plate 7). The 'welding rod' tracks through the hand piece (plate 8) at a rate that approximates to real welding. One pass of the track takes approximately 1.2 mins. Any deviation of the rod from the track is recorded as an error score on the counter (plate 6). The track itself can be raised or lowered to any required height and tilted 90° through any plane.

4.0 PLAN FOR 12 MONTH PERIOD ENDING MARCH 1976

(i.e. first year of Part II of this project Convention: 6245. 35/8/002)

4.1 Laboratory Studies

- a) effects of posture in manual metal arc welding. Parameters being measured include heart rate, EMG, energy expenditure and subjective estimates of fatigue.
- b) carefully controlled experiments to quantify changes in EMG/spectrum relative to frequency, percentage of maximum voluntary contraction and duration of contraction.



a) Welding gun and rod

b) Battery box

Plate 5 - Welding simulator complete with stand

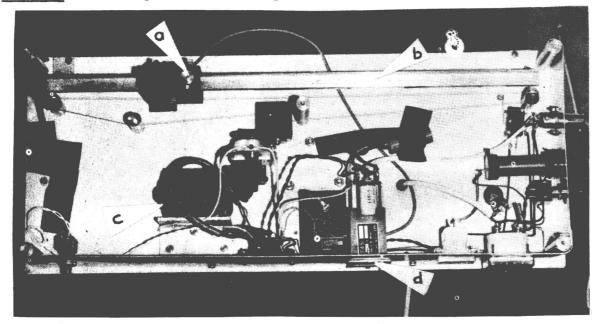


Plate 6 - Inside of welding simulator

- a) Photoelectric cell and carriage
- b) Carriage track
- c) Drive motor and gear box
- d) Error counter

1248/76 e - ACE

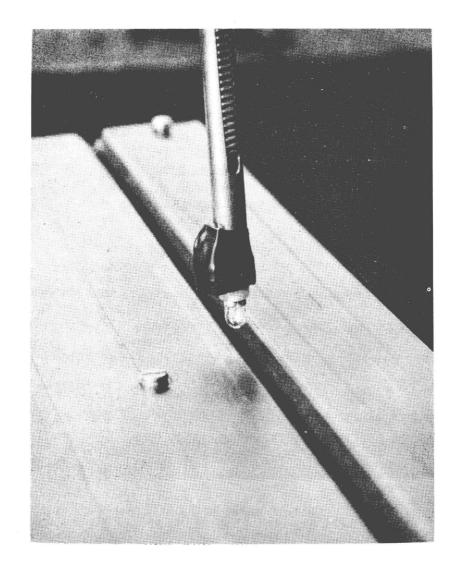


Plate 7 - Close up of track and end of 'electrode' showing small bulb used to activate the photocell

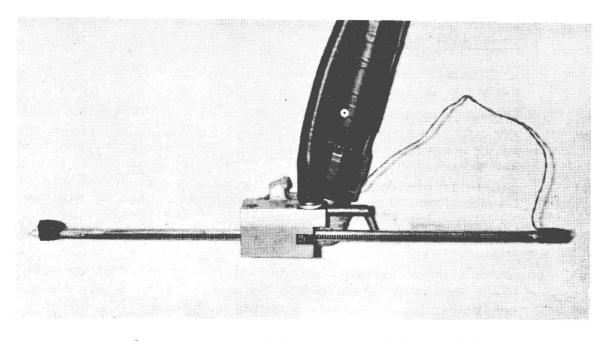


Plate 8 - Modified welding gun and 'electrode'

- c) determination of suitable sites for body temperature measurement.
- d) production of hardware for collection of EMG data on site using miniature tape recorders.
- e) consideration of further simulation studies.

4.2 Field Work

- a) Exploratory and follow up studies of industrial welding tasks.
- b) Exploratory and follow up studies of coke-oven workers.
- c) Investigation of other industrial tasks for future study.

5.0 APPENDICES

5.1 APPENDIX I - CRYSTAL TIMER CIRCUIT DESCRIPTION

The timer is built around the SAJ 220S monolithic integrated circuit made by ITT. It comprises an oscillator circuit, fifteen divider stages, a pulse shaper, a driving circuit and a stabilising circuit. A schematic diagram is shown in Figure 1.

The circuit uses a quartz crystal for precise control of the operating frequency of the circuit. The crystal frequency is 32.768 KHZ. When using a crystal operating at this frequency the output stage supplies monopolar pulses with a repetition frequency of 1 Hz and 32 ms duration. This was the exact repetition and duration required.

The oscillator circuit diagram (Figure 2) shows the components mentioned and the other biasing stabilising components. The diodes used as a voltage dropper.

The oscillator output waveform is shown in Figure 3. The required waveform is the inverse of this and therefore an inverter was added to the circuit.

In this circuit (Figure 4) the transistor acts as a switch. The tape head is connected between O_{ψ} and the output terminal. When the transistor is switched off the collector to emitter impedance is high

compared to that of the tape head and current flows through the tape head. When the transistor is switched on the collector to emitter impedance is low compared to that of the tape head and the current passes through the transistor.

The transistor is on during t_r and off during t_d .

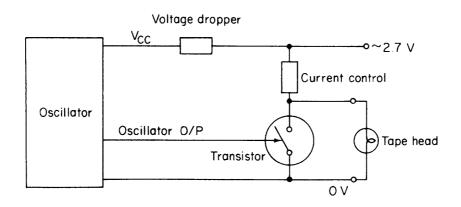


Figure 1 - Schematic diagram of timer

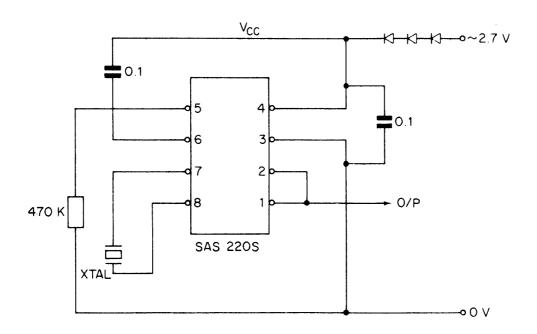


Figure 2 - Oscillator circuit

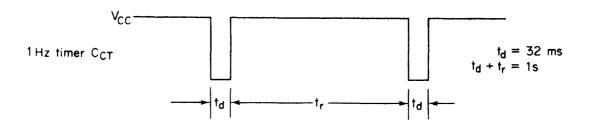


Figure 3 - Oscillator output waveform

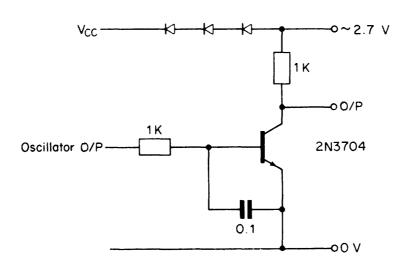


Figure 4 - Inverter circuit

5.2 APPENDIX II - DESCRIPTION OF ACTIVITY CODING DEVICE

The basic component block of the activity encoder are shown in Figure 5. The keyboard has sixteen keys of which only one may be pressed at any one time. There are sixteen signal lines which carry the keyboard information (one line for each key) to the next part of the circuit, which is the 16 line to 4 line BCD converter.

The sixteen signal lines are fed into two eight-to-three-line priority encoders. The lines are normally held high by pull-up resistors and when a key is depressed the appropriate line will carry a low-signal. The signal will be converted to a three bit binary code and the MC 14528 (one-shot) will receive a signal indicating that a key has been depressed.

The three bit binary output from each priority encoder is fed to a set of three NAND-gates. Using the priority encoders and the NAND gates the keyboard inputs can be encoded into four bit BCD (Figure 6).

The outputs from the NAND gates are fed into a quadruple D-type batch and this is clocked by the output of the one-shot. This staticises the data and if the data was not batched then when the key is released the output will be indeterminate.

The four bit output from the batch is then passed into the display and into the output driving stage.

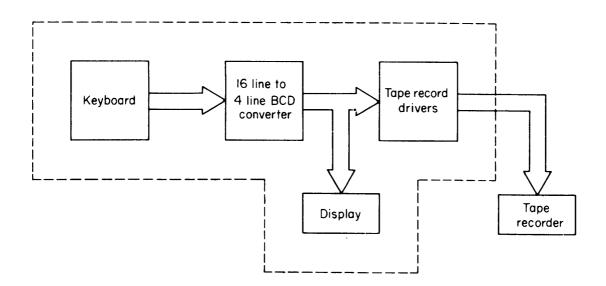


Figure 5 - Activity encoder AE-1-Block diagram

The display stage (Figure 7) consists of a binary to seven segment converter and a liquid crystal driver. The display device is a HAMLIN liquid crystal display. The clock that generates the a.c. waveform to drive the display is located in the binary to decimal conversion part of the circuit.

The output driving stage (Figure 8) consists of a set of inverters, a pair of summing amplifiers and an amplifier which generates a reference voltage VREF.

The four bit output from the batch is in the wrong sense and so the inverters are used: the four bits are then summed in pairs and when the reference voltage is fed into the non-inverting inputs of the amplifiers the outputs A and B are coded as follows: -

Key Depressed	A(mV)	B(mV)
0	- 50	- 50
1	- 25	- 50
2	+25	- 50
2 3 4	+50	- 50
4	- 50	- 25
5 6	- 25	- 25
6	+25	- 2 5
7 8	+50	- 25
8	- 50	+25
9	- 25	+25
10	+25	+25
11	+50	+25
12	- 50	+50
13	- 25	+50
14	+25	+50
15	+50	+50

An interrupt (INT) output is also produced. The signal originates in the one-shot and is used to indicate that a key has been depressed.

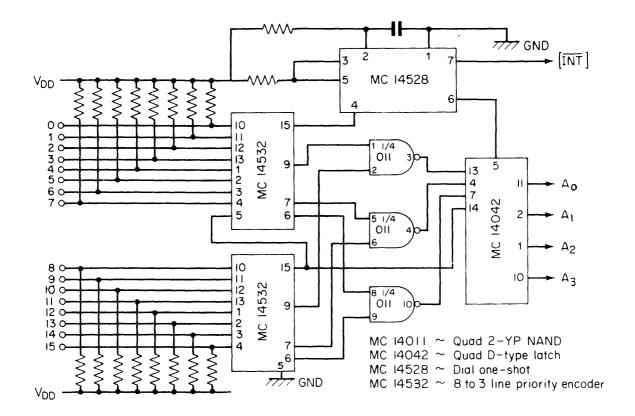


Figure 6 - 16 line to 4 line BCD converter

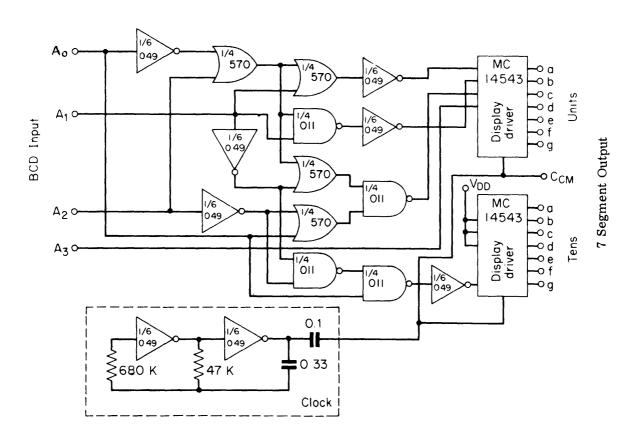


Figure 7 - Display circuit

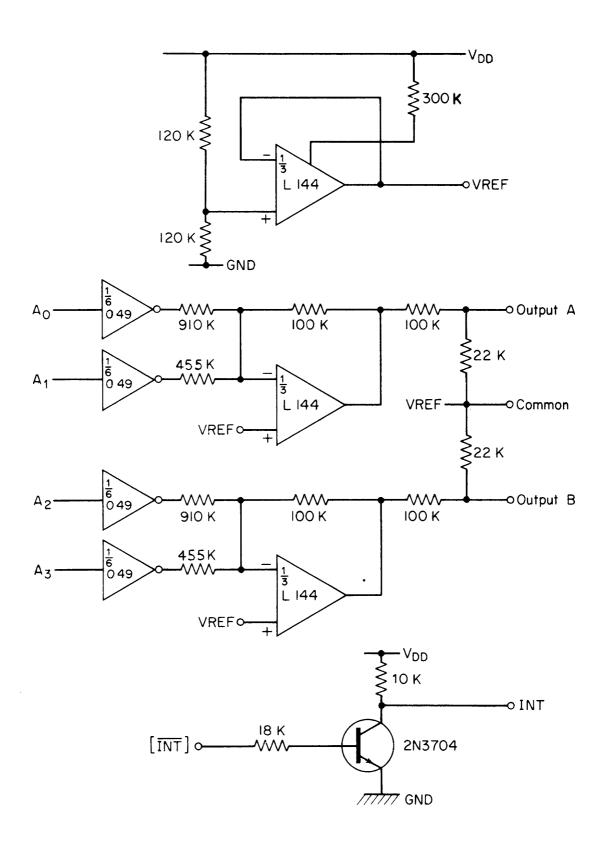


Figure 8 - Output drive circuit

5.3 APPENDIX III - HEART RATE DATA COLLECTION AND ANALYSIS

INTRODUCTION

The system described in brief in the main text of the report is here described in some detail. The system is used in both laboratory and working environments. A schematic diagram of the complete system is shown in Figure 9.

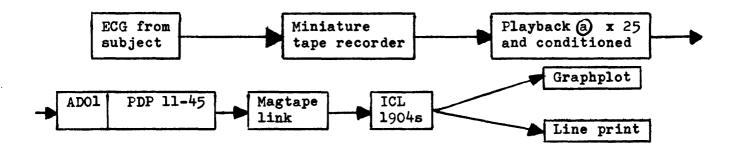


Figure 9 - Schematic diagram of complete heart rate system

Data Acquisition

See main text.

Analogue to Digital Sampling

The cassette containing the ECG and timer recording is played back into an ADO1 analogue to digital sampler on a PDP 11-45 computer operating under the DOS system.

Sampling takes place at 2000 times per second (once every 500 microseconds in real time). Because of this high sampling rate 70 % of the computer's processor time is used during sampling, and hence any calculations on the data are impossible until sampling has finished. Because of this limitation all statistical analysis and further calculations are performed on the larger 1904s computer.

The ECG signal is conditioned by a pulse interval timer unit (PIT) before playing into the ADO1. This unit produces a 20 volt spike for each QRS complex recognised in the new ECG signal. The PIT output is alternated to approximately two volts before inputting to the ADO1.

Before playback is started, threshold levels for the PIT signal and timer are selected by preliminary examination of the trace on an oscilloscope. These values are typed into the computer from a terminal. They are chosen by ensuring that every pulse is at least as wide as the sample to sample interval (i.e. 500 μ sec) at the threshold voltage. This ensures that each pulse will be sampled at least once.

In the sampling process the times at which each signal is above threshold are stored on disc in the form of double precision words, all times being stored in "computer clock units" (100 μ sec units). Normally this means that about 100 000 items have to be stored for an eight hour recording. The timer and ECG/PIT channels are differentiated by assigning negative values to the timer and positive to the ECG/PIT. At the end of a run information is transferred from disc to magtape which is used as the transfer medium between the two computers.

Initial Analysis in the 1904s

This part of the system produces inter beat interval (IBI) data from the information on the magtape. This is achieved by the FORTRAN program BREN which is outlined in Figure 10. The program consists of four main stages as described below.

(i) Input

Data input from magtape is read a block at a time and converted from PDP 11 double word integer format to ICL floating point.

(ii) Removal of retriggering

Surplus data is collecting in the sampling procedure for both the timer and ECG channels, for there may be more than one sample per pulse at which the signal is above threshold. This is termed retriggering. Simple algorithms can be used to eliminate this, and these are described below.

(iii) Calibration

Heart rate IBIs are calibrated every 5 secs with reference to the crystal controlled timer signal. This is done by calculating the "speed-up factor" every 5 secs through the run. The speed up factor is defined as below: -

speed up factor (SF) = $\frac{\text{replay speed}}{\text{record speed}}$

(iv) Noise detection

The aim of this is to identify where noise occurs through a run, and to substitute interpolated values at these points. Although this may seem to be a dubious procedure on theoretical grounds, in practice it works well as most periods of noise are of short duration.

Initially there is a search for the first time pulse for this defines the start of the run. Provided another time pulse follows this one within $35.7 \rightarrow 66.7$ m secs (i.e. allowing for a maximum variability in speed up factor of times 15-28) this first time pulse is taken as the start of the run. The program then scans for further time pulses which are accepted of the time pulse gap between the time pulse under consideration and the previous pulse lies within -5% to +15% of the previous gap. Any input time item which does not pass this test is rejected and assumed to be due to retriggering of the time pulse.

In practice it was found that occasionally "drop-out" occurred on the tape so that a timer pulse was missed completely. In order to allow for this, if the first test had been exceeded a second test was applied. If a time pulse gap is found to be within $\frac{1}{2}$ 15% of time the previous gap then it is assumed that a time pulse has been lost.

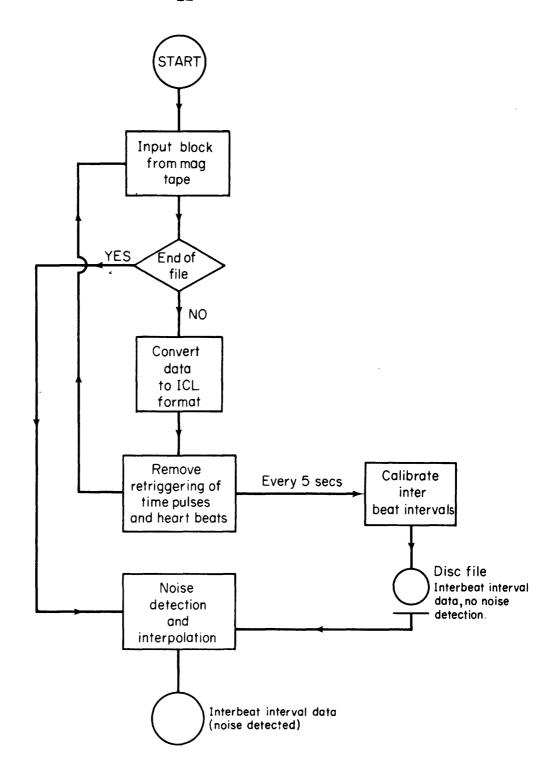


Figure 10 - Flow diagram of program BREN

If at any stage of the program both of these tests fail then the program is terminated.

Every 5 secs (that is every 5 timing pulses) the speed-up factor is calculated from the formula

SF =
$$\frac{5000}{T_6-T_1}$$
 (where T_6 and T_1 correspond to the times in any 5 sec period).

This speed up factor can then be used to calibrate the inter beat interval data. Retriggering of the ECG data is done by only accepting R waves if the gap between the one under consideration and the previous one is longer than 7 m sec (corresponding to a heart rate > 200 at a max SF of 28) once retriggering has been eliminated uncalibrated inter beat intervals can be calculated by subtracting the time of the previous R wave from the R wave under consideration. Calibrated inter beat intervals are then calculated by multiplying the uncalibrated values by the speed up factor. Calibrated interbeat interval data is stored on disc file before noise detection.

In the final part of the program, interpolated IBIs are substituted for values which are likely to be incorrect due to noise. Noise is defined in terms of an inter beat interval which fails to meet one or both of the criteria below

- (i) an IBI must lie between 300 and 1500 m sec
- (ii) successive IBIs must fall within a certain range of each other. In particular ${\tt IBI}_{\tt I+1}$ must lie in the following range of ${\tt IBI}_{\tt I}$

$$(2 \times IBI_{I}) -290 > IBI_{I+1} > (0.7 \times IBI_{I}) + 90$$

These criteria were chosen because they were simple and could be easily changed if experience indicated they were incorrect.

Recovery from noise occurs when four consecutive interbeat intervals pass criteria (i) and the last three pass criteria (ii). This is the minimum number of beats for recovery to be logically certain based on the two criteria. Once recovery has been effected interpolated values are calculated.

The number of beats lost during noise (N) is estimated by :

N = nearest integer $\frac{t}{IBI}_{mean}$ where IBI_{mean} is the average of the last legal IBI before noise and the first legal IBI after the noise. t is time noise lasts

The N interpolated IBI values (IBI $_{TNT}$) are then defined by :

$$IBI_{TNT} = \frac{t}{N}$$

Finally criterion 2 is used to check the legality of recovery, i.e. to check that the IBI can change from pre to post noise levels in the time t. The noise state is re-entered if this recovery is illegal.

Final Analysis on the 1904s

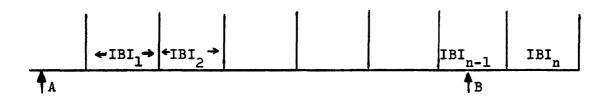
Analysis of the IBI data is achieved by PROGRAM HEAR which is outlined in Figure 11. Interbeat interval information (from program BREN) is input, together with information as to activity types and their times of onset. The program produces an analysis of the data for each activity in turn, and then for all similar activities. A graph plot is produced showing the heart rate to a resolution specified by the experimenter. Examples of a typical output showing all the parameters calculated is shown in the supplement to this Appendix.

The exact definition of the quantities calculated is as follows:

(i) Heart rate calculations

Wherever heart rate is calculated between two points A and

B (e.g. ½-1 min heart rate, heart rate over any activity, heart rate every six secs) the following method is used:



Heart rate beats/min A-B = $\frac{N}{N}$ x 60 000 where IBI values are in m sec $\sum_{k=1}^{\infty} IBI_k$

(ii) First and last 10 beats calculations

$$\frac{HR_{lst ten beats} = \frac{10}{10}}{\sum_{k=1}^{10} IBI_{R}} \times 60 000$$

HRlast 10 beats =
$$\frac{10}{\text{na}}$$
 x 60 000 (m beats in an activity)
$$\sum_{k=n-9}^{\text{HBI}_{R}}$$

(iii) Max HR

Defined as the max serial 10 beats

i.e. Max
$$j+a$$
 x 60 000 where j takes all values from 1 to m-9 (m beats in an activity)

Cardiac Cost Calculations

A value HSTAR is typed in in beats/min and all calculations are based on this.

Card cost = no. of beats where
$$IBI_k > \frac{60\ OOO}{HSTAR}$$
 for all values of k from 1 to m

card cost time =
$$\sum_{k=1}^{n} IBI_{k}^{x}$$
 where $IBI_{k}^{x} = IBI_{k}$ if $IBI_{k} > \frac{60\ 000}{HSTAR}$

$$IBI_{k}^{x} = 0 \text{ if } IBI_{k} = \frac{60\ 000}{HSTAR}$$

 $card cost/min = \frac{card cost}{card cost time}$

Accuracy and Testing of the System

The system has been carefully checked by comparison of simulated data (created using a pulse generator) and chart recordings of 'real' data with the analysis output. No discrepancies of 'real' with computed data were found.

The accuracy of the system is limited by the sampling method. For six second heart rates the experimental error was approximately - beats/min at 180 beats/min and - ½ beat/min at 60 beats/min.

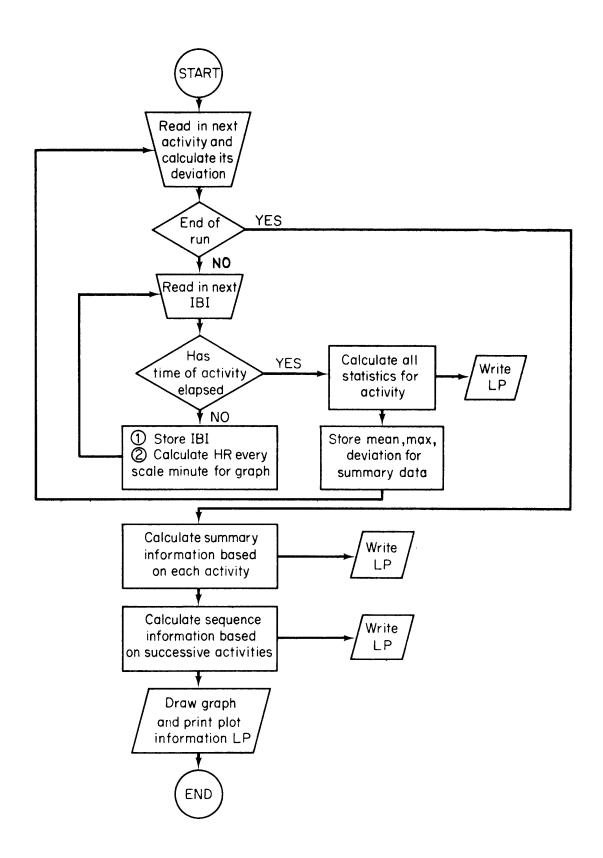


Figure 11 - Flow chart of program HEAR

SUPPLEMENT TO APPENDIX III

EXAMPLE OF COMPUTER PRINT OUT

- i) Input data (i.e. data produced from PDP 11/45 sampling procedure)
- ii) Calibration periods.
- iii) Noise detected.
- iv) IBIs with noise.
- v) IBIs without noise.
- vi) Summary sheet of mm length, speed up factor, and noise detected.
- vii) Heart rate data for individual activities.
- viii) Summary heart rate activity for all activities.
- ix) Graph information.
- x) Sequence information for heart rate.
- xi) Sequence information for activities.
- xii) Graph plot.

31661.	31716.	31786.	31991	32206.	32421.	32626.	32836.	33051.	33266.	33621.	33896.		0 4		35336.	-		-	36381.	36651.	36871.	37086.	ā,	37696.	37911.	35120.	1676	39096	39311.	39791.	40136.	. 90707	. 12904	.0030	61661	41656.	42001.	42229.	1979.		43346	43566.	4.39.24.	44101.	44406.	44756.		45454		46091.
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ii) Calibration Periods

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248/76 - ACE

iii) Noise Detected

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iv) IBIs with Noise

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-	44.18	•	1 454.55	1 K. 838 1	1 02.076		1 641.18 1	٩.	. 497
	441.24	6,8717	59.767	00000	1 54. 45		1 59. 767	4.8965	. 84 . 84
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	100 247	•	, CB 7	7 0081	00 077	•	66.6		997
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-	1 54.357		16.742	1 7,1004 1	54. 767		0.	٠.	441
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v) IBIs without Noise

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1	571.23	4006	585,11	5010.7	- 1824	9446	574.81	7620.7	558.51
7 7 8 8 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4 4	571.41		1005	2500.5	00.079	5.0159	00.000	5.0259	443.3
5,0834	A07.00		574.84	6,0556	560.00	5.0650	1 860.00	5,0763	5.66.6
- 40	518,62		518.67	5001.5	548.62	5.1094	518.62	5.1180	505.4
	70° C67		40.50	5785	20,267	5 1927	20.24.7	5.2007	707
5_20R9_1	478.72		478.72	5.2248	478.72	5.2328	478.72	5.2408	4.87
5.74.88	444.47		446.67	5,2643	152,257	5.2719	1 451,11	5.2794	451.1
2.2869	451.11		1 11 11 1	2101.5	1 11 157	5.3095	1 11.157	5.31.0	9.997
5 4248			72.24	8055.	650.037	5.5472	458.85	5,5543	6.02
5 4986	01 08 7		4 30 10	5.17.5	61.057	5.4205	4 39 49 4	5.75	0.033
2517.5	24.457	5.4427	100.077	9697, 5	1 00.077	5.4570	1 00.077	2.4643	9.927
5.4714	ີ ເປ ິບ27		430.00	8587.5	00.027	6267.5	1 00.027	5.5001	0.077
7,000	00.033		126.67	5.524	10.75	2.579	1 00.077	00000	9.927
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1 7677 5	113.54		1 29 927	7197.5	26.217	5.6703	1 777.76	5.4772	7.717
5.4861	77.747	5 4014	17.747	1464.4	82.767	5.7050	1 417.78	2,7,2	7.00
5.75%	484.62		1 29 227	2649	411.14	5.7737	72.607	5.7806	2 607
5.7874	72.007		77.607	4.8041	72:607	5.8079	1 72.607	5.8147	4.607
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0068.5	40.007		40.604	2,00,5	90.607	5.940.5	90.607	5.0173	0.607
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5.9582	104.51		404.51	4.07.3	1 15. 707	8.9784	1 411.14 1	5.9853	197.8
7520.9	20.00	5.00.84	412.51	4.0004 4.0004	308704	2670	412.23	6.0528	5.67
4.0507	411,11		411.11	71 20 7	411,111	6.0802	1 16,916	A.0871	6.11
6.7949	411.11	A 100k	66.667	1 1077 1	66.667	6.1145	1 66.967	4.9.9.4	1.767
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6.2325	414.89		416.89	4.2649	412.71	6.2530	1 426.67 1	4.2601	
- 200.0	00.057			2010	00.087	A 2005	- 00.004	4000°	445.55
6 4481	427.81		41 454	4 3525	91, 917	4508	446.464	A . 46.70	
6, 1743	434,16		436.14	4. 4688	91. 427	4.3961	436.16	4.4034	· ·
1 7067. 4	K5.22	6.4964	613.35	1 2527.7	1 55.017	4.4322	1 55.617	4.4392	5.667
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	419.55		410.54	A.5301	410.25	6.5379	419.55	4.5469	- 0
•	4 8 8 7 E		452.13	1 6595.7	1 87:597	A.5737	1 452.13 1	4.5812	57.
•	94.727		457.64	1 1704.4	25.53	6.6116	453.31	A. 492	53
•			455.55			, , , , , , , , , , , , , , , , , , ,	- AC	0,64.4	•
A 7036	,		1 25 557	0012.4	455.33	4,7265	440.00	4.7330	
	1 54.057		458 AC 1	1 27543	458" AS 1	4.7644	1 458.85	4.7720	•
1 2022.4	452.45	A. 7872 .	458 XS 1	0562.7	1 S8 857	4.8024	1 658.85 1	4.8102	757

1248/76 e - ACE

vi) Summary Sheet of mm Length, Speed Up Factor and Noise Detected

STANALY SHEET FOR HUN, 2 P19

I FIGTH OF DUP BETTE FALIERATION : 477,750MINS
FOODEX AMOUNT OF UNFAIJPEATED DATA AT FIND OF RUN : 45ECS
90FECTIF FACTOR PAPOR: 74,042 - 27.322

TI'S LUGT EGTAPLIGHING INITISL HFART STANDARM : N. 1769ECS

MFAN COFER-UP FACTOR : 24.891

IFFGTH OF PIN AFTER ACTSF DETECTION : 477,750MINS
TOTAL TIME (F WISE DETECTED : 0,793MINS
DEDCT-TAGE OF MISE DETECTED : 5,500%

vii) Heart Rate Data for Individual Activities

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_	140.2		4 5 5 5 5 5 5 5 5 5 5 5 5 5 5 5 5 5 5 5	44. 4. 4. 4. 4. 4. 4. 4. 4. 4. 4. 4. 4.	136.3 103.0 118.1 122.4 133.2 115.8 115.8 117.2 117.2 117.2 117.2 117.4 117.2 117.4 117.2 117.4
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0 . 9 . 9	• • • • • • • • • • • • • • • • • • • •			14.7 1 12	117.0 114.0 128 122.4 122.7 128 115.8 112.8 123 100.1 86.4 123 117.2 113.4 123 105.9 90.0 124 108.0 105.4 115
4 1 124.6 1 0	124.4		25	112.8 128 112.8 128 113.6 128 90.0 124 115.6 118	122.4 172.7 128 115.8 112.8 123 100.1 86.4 123 117.2 113.4 123 105.9 90.0 124 108.0 116.6 116
.6 1 116.7 1 0	122.6	* * * *		172.7 172.8 142.8 172.9 143.6 172.9 105.6 116	115.8 112.8 128 100.1 86.4 122 117.2 113.4 122 105.9 90.0 124 108.0 105.4 115
.7 124.8 1 9.	122.7	K 4 4	12 2 2 2 1	46.4 123 113.4 123 90.0 124 115.6 116	115.8 112.8 123 100.1 86.4 123 117.2 113.4 123 105.9 90.0 124 108.0 105.4 115
.7 ! 114.4 ! 0	121.7	4 4	2 2 2 1	86.6 122 90.0 124 105.6 116	117.2 113.4 1128 105.9 9n.0 124 108.0 175.4 115
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.1 119.4 1 0	105.1	٠,	4.05.9 1 116.5	- -	1 105.1
.3 146,4 1 0.	126.3	4.	126.3 1 140.4		1 126.3 1 164
.3 148.1 0	147.3	·	147.3 i 168.1	 r	147.3
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	162.4			- 1 38 4	1 0.45 1 132.6 1 128.4 1 142.6
. 129.0 1 0.		٠,			

viii) Summary Heart Rate Activity for All Activities

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deskkedstr		118.1	1 7.01	0,34	0.24	Ç.	11117.52
ocal decemb		11 120.0	· · · · · · · · · · · · · · · · ·	0,34	0.4	.	110.68
\$11/5TNDCA11		110,1	10.7	1.85	2.49	22	49.59
AFELES VACE	٧	127.2	# , ac	0.21	0.15	~	11 R2.43
7/18/A 17/6		11 122.6	7.6	0.10	9.45	;	91.47
sull dealest	~	1,77,1	1 5.2	47'0 -	64.0	•	1114.06
sull espec	· · · ·	152.7	· · ·	0.34	0.00	er	1132.49
V	<u>:</u>	11 124.3	· · · ·	1 0.5R	¢	•	1124.89
ارد لايم	.	11 188.3		1 0.23		.	11133.92
	<u>}</u>	141.5		1.38		.	1161.44

THE WELL LEADT SATE THE WHOLE PERING WAS 104,5856BEATS PER MIN

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ix) Graph Information

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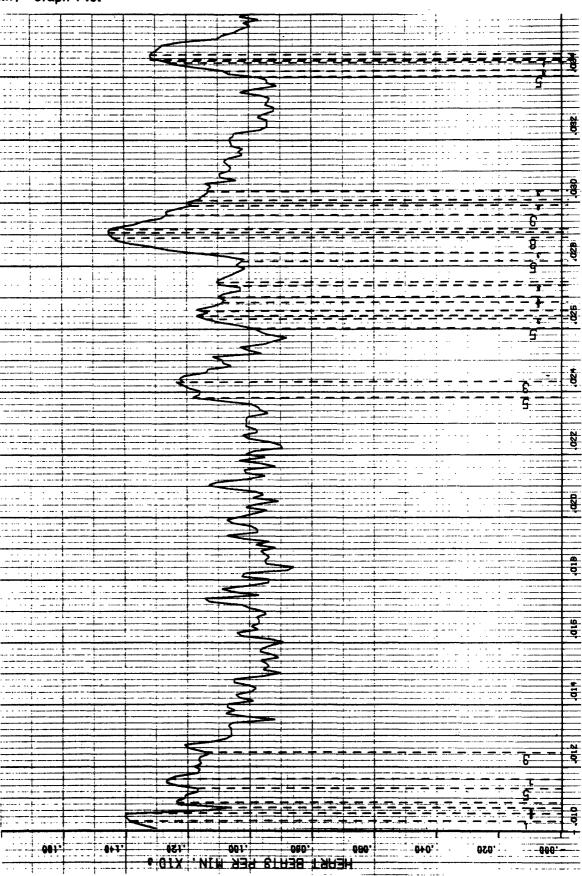
x) Sequence Information for Heart Rate

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PILL VALVE "	c 	•	· · ·		c	· ·		c	0	~	c	•
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xii) Graph Plot



5.4 APPENDIX IV - SUBJECTIVE RATINGS OF FATIGUE

Indications of fatigue are obtained during laboratory experiments by

- a) ratings of local and general fatigue given by a pointer test.
- b) relative comfort of different body parts by a forced choice ranking test.

Local and General Fatigue

A modified Bujas method was used to get rankings of local and general fatigue before, during and after the work tasks. The free scaling method of Bujas was not employed due to the lack of maximum values. Instead of the free scaling method the pointer method of Hueting and Sarphati was adopted. Subjects were asked to rate their feeling of fatigue by adjusting a pointer to the relevant place on a 14 point scale. One end of the scale was labelled "not at all tired" and the other "absolutely exhausted". There were two tests of this type, one for local and one for general fatigue. It was found as suggested by Bujas that subjects could readily differentiate between these two categories.

Test for Relative Comfort of Different Body Parts (Forced Choice Ranking Test)

This test was added to the previous two to get an idea of which parts of the body became most uncomfortable during work. A diagram of a man is shown with 15 parts of the body outlined (see Supplement 3, Appendix V). The subject is asked to pick out the 3 parts of the body that are the least uncomfortable. Once this has been done the subject picks out the next 3 from those remaining and so on. The design of this test comes from work on seat comfort⁹.

5.5 APPENDIX V - QUESTIONNAIRE AND FATIGUE RATINGS FOR WORKS BASED MEASUREMENTS

Purpose of the Questionnaire

- 1. To broaden the project so that not only physiological parameters are considered when recommendations are made about work organisation.
- 2. To compare physiological data with subjective reactions to different tasks, both on an individual and on a group basis.
- 3. To provide information which together with productivity measures etc. could be used as evaluation criteria in a post-study follow-up.

The questionnaire is divided into two sections in order to prevent respondents becoming bored by having to answer too many questions at one time. The first section covers personal details required for cross-reference with physiological data, on an individual basis and also in conjunction with epidemological information from the industry. In addition there are two questions on subjective fatigue.

The second section asks for information about, and attitudes towards, the current work situation, the standard of protective clothing available and the prevailing environmental conditions.

Besides the basic questionnaire, however, three other measures have been developed. Two of which relate to physical fatigue and the third to "mental" fatigue. Allthree measures are taken at the beginning, middle and end of the shift. Thus changes in fatigue can be monitored over the day.

PART ONE

As far as possible the only answer required in both sections of the questionnaire is a cross in the relevant box. The intention being to allow respondents to work through as quickly as possible. The first nineteen questions of section one are concerned with general background and personal information needed for cross-reference with physiological data.

The final two questions relate to subjective fatigue and it is hoped that individuals' answers to these two will relate well to the repeated subjective fatigue measures.

Questions 1-8, 12-15 and 20-21 do not have to be modified before they can be applied to different jobs.

Questions 9-11 and 16-19 do require modification for different jobs.

A sample part one of the questionnaire is contained in Supplement 1.

PART TWO

Questions 1-7 relate to the concept of job satisfaction which is important because any successful work reorganisation must take employee satisfaction into account.

Question one asks for a straightforward statement of level of job satisfaction. The statements used were generated by Bibby 10 and have already been found to differentiate well between indiviuals.

Question 2 serves as a back-up to the above and answers will indicate which kinds of jobs different individuals see as satisfying and why.

The third question rates jobs along a number of dimensions considered to be important in promoting job satisfaction. Generation of a "job profile" from this question should highlight areas in need of improvement and/or reorganisation. A post-study evaluation will test the success of any recommendations made by producing more favourable answers to this question.

Questions 4-7 continue to rate job satisfaction in greater detail concerning the dimensions of individual autonomy and amount of feedback from superiors. Again a post-study evaluation of the success of any reorganisation measures should be reflected in answers to these questions.

Question 8 asks about the working environment.

Questions 9 and 10 list the items of protective clothing available for use in any particular job, so unlike the previous eight questions, these two vary according to the job being studied. The aim of these two questions is to find out what individuals commonly wear and also to spotlight any flaws in design or quality of any particular piece of equipment from the employee's point of view. Feedback from these two questions could possibly go a long way towards improving safety at work, as well as promoting satisfaction.

Finally, Question 11 invites further comments about the topics considered in Section Two, in the hope that any missed points, felt to be important by the people who actually do the job will be brought to the project team's attention.

A sample questionnaire is contained in Supplement 2.

Repeated Subjective Fatigue Measures

There are three tests for rating fatigue. The rationale underlying these three measures is that there is fatigue which is not easily measured physiologically. That is, there are <u>subjective feelings</u> of both physical and mental fatigue. Two of the tests have also been used in the laboratory studies and their methodology is reported elsewhere.

Only one of the tests, however, the Forced Choice Ranking Test, has been incorporated into the field work methodology without modification. As in the laboratory respondents are shown a diagram of a man, on which 15 parts of the body are labelled. They are then asked to pick out the three most uncomfortable parts of their bodies, then the three next most

uncomfortable etc. until all 15 parts have been chosen. Answers are recorded on a separate scoring sheet, (see Supplement 3).

The second test originating from the laboratory studies has been modified in that respondents are no longer asked to move pointers to indicate levels of local and general fatigue. Instead they are asked to mark the point on a 10 cm line (after Osgood et al 11) that best indicates how tired they feel, both generally and in the muscles being monitored by the EMG recorder. In addition, respondents are asked to state how long they feel they could continue with what they had just been doing before feeling completely exhausted.

The third subjective test concentrates on "mental" fatigue and is based upon the Nowlis Mood Adjective Check List (MACL)¹². The MACL, however, merely presents a list of adjectives to the individual who then has to indicate the strength of his present feelings.

This was not felt to present enough "structure" to the respondent for the purposes of this study, therefore a bipolar approach was adopted, after the form used by Vogt 13. The box matrix used by Vogt was, however, rejected in favour of the 10 cm line method used in the previous test, because it was felt that having used that method of responding once, subjects would find it easy and quick to apply here.

Altogether, 26 adjectives from the Activation-Deactivation Adjective Check List derived from the MACL by Thayer 4, were selected and formed into 13 pairs of favourable/unfavourable state adjectives, for use in this study. Positive and negative poles were randomised in an attempt to prevent subjective response sets developing.

Scoring for this test, and the second of the two laboratory tests, will involve assigning 0 to the positive pole and 10 to the negative pole,

with intermediate values depending upon the distance along the 10 cm line. Correlation matrix and linkage analysis programs (Bibby 10) will be used to identify clusters.

The overall aim is to find out whether there is more than one component to fatigue. All three subjective tests are applicable as they stand, to any group of workers. A sample scoring sheet for the Forced Choice Ranking Test and the two other tests, as presented to respondents are included in Supplement 3.

SUPPLEMENTS TO APPENDIX V

Supplement 1 - Questionnaire

Supplement 2 - Questionnaire

Supplement 3 - Subjective estimates of fatigue

SUPPLEMENT 1

The study that you are involved in is being carried out by BSC staff of the Corporate Engineering Labs at Battersea.

The study us designed to investigate how fatigue develops in the human body during working hours. As you already know, we are collecting measures such as heart rate by using personal miniature tape recorders. Similarly your activities are being recorded so that we can relate these to changes in your heart rate.

In order to have all the information that may be relevant to your feelings of tiredness, we have devised a simple series of questions which one of our team will ask you at some point during the shift.

These questions fall broadly into three groups :

- 1. Personal details
- 2. Subjective fatigue i.e. how tired you feel
- 3. Job related factors i.e.
 - a) How various parts of the job affect your feelings of tiredness.
 - b) Your opinions, as the person who actually does the job, of the way it has to be carried out.

NOTE

Individuals' answers to these questions will be treated as confidential to members of the investigating team. General conclusions from the whole study will be made available as soon as possible.

Finally - without your help this investigation would have been impossible. On behalf of the whole team, I would like to thank you for your patience and co-operation.

John MUSGROVE

1)	Name		• • • • • • • • • • • • • • • • • • • •
2)	Date of Birth	• • • • • •	• • • • • • • • • • • • • • • • • • • •
3)	Marital Status		
			Married
			Single
4)	How many dependent children do you h	nave? .	
5)	How far do you travel to work?	• • • • • •	miles approx
6)	How long does it usually take you to	get to	o work?mins/hrs approx
7)	How do you travel to work?		
			Walk
			Cycle
			Motor Cycle
			Car
			Public Transport
8)	Do you smoke?	-	
			A pipe
			Cigarettes
			Cigars
	b) If yes, approximately how many co	igarett	es/cigars/ozs of tobacco
	do you smoke per day?	• • • • • •	• • • • • • • • • • • • • • • • • • • •
9)	Do you suffer from eye strain		
	after welding?		Yes
			No
10)	Do you ween spectages		
T ()	Do you wear spectacles?		
			Yes
			No

	b) If yes, do you wear your spectacles while welding?	
		Yes No
11)	Do you wear contact lenses?	
		Yes
		No
	b) If yes, do you wear your lenses while welding?	
		Yes
		No No
12)	Do you generally use?	
		Left hand
		Right hand
		Use Either
13)	Do you have any regular spare time activities or hobbies	which involve
	physical exercise?	
		Yes
		No No
	b) If yes, what are they?	• • • • • • • • •
	c) Approximately how much time do you usually give to the each week?	-
14)	How long have you been employed by BSC?year	rs
15)	Did you work in the steel industry before nationalisation	1?
		Yes No
	b) If yes, for how long?years	

16)	How long have you been a welder?years
17)	Have you ever attended a formal training course in welding?
	Yes
	No
	b) If yes, were you sent on this course by an employer?
	Yes
	No
	c) How long did the course last?
	d) Was any recognised qualification awarded at the end of the course?
	Yes
	No
	e) If yes, what was the qualification?
- 0 \	
18)	What other, if any, qualifications do you have in welding?
101	Is there a regular test of welding ability that you have to take?
19)	Is there a regular test of welding ability that you have to take?
	No res
	b) If so, what is it?
20)	At the end of a shift do you usually feel??
	More physical than mental tiredness
	More mental than physical tiredness
	About the same

21)	At the end	of a working	g week do you	usually	feel more	tired	than
	you did at	the end of t	the first day	of that	week.		
							Yes
							No
	b) If yes,	is this tire	dnes	• • • • • • •	?		
			more phys	ical thar	n mental		
			more ment	al than p	physical		
			about the	same			

SUPPLEMENT 2

The following questions are concerned with opinions about job and working environment. All answers will be treated as confidential to the project team so please feel free to give unfavourable as well as favourable opinions. The purpose of this section is to find out the opinions held by welders, as a group, not to identify individuals.

Please read each question carefully and try to answer them all. If you would like to make any additional comments please use the space provided at the end.

1)		your feelings about your job.
	A	This job isn't very far short of what I would consider to be ideal from my point of view.
	В	Although it's not ideal the advantages certainly outweigh the disadvantages in this job.
	с	Although, taken all round, my job is all right, there are quite a few things which I consider important, that are wrong with it.
	D	I don't get very much out of this job compared with what I really want from it.
	E	I think this job is terrible - if I had a choice, it's about the last job I would choose to do.
2)	Have you	had any other jobs that you preferred to welding?
		Yes

Ъ) If yes, what we	re they?	• • • • • • •	• • • •	• • • • • • •	• • • • • • • • • • • • • • • • • • • •
	••••••	• • • • • • •	• • • • • • • •	• • • •	• • • • • • •	
С) Why did you pre	fer them	?	• • • •	• • • • • • • •	• • • • • • • • • • • • • • • • • • • •
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	lease try to desc	·-	r particul	ar j	ob in rel	lation to the
8	tatements given b	elow.				
	٢		Neither]
		True	one nor other	the	True	
	he work is nteresting					The work is un- interesting
	_		<u> </u>			1
	Γ	Mm	Neither			
		True	one nor other	the	True	
	romotion pro- pects are poor					Promotion pro- spects are good.
	1					
		True	Neither one nor other		True	
Un a	employment is constant threat				***************************************	Employment is secure
	L		<u> </u>			J
	Г		Neither		····	1
		True	one nor other	the	True	
	ere is close					There is little contact with
	rkmates					workmates

		Neither the		1
	True	one nor the other	True	1
Good work is al-		Ovici	 	Good work is never
ways appreciated				appreciated
Į.			<u> </u>	J
i		Neither the	 	7
	True	one nor the	True	
		other		j
Each person has responsibility for his own work				Each person does not have responsibility for his own work
101 110 0111 110111 1			<u></u>	J 101 M15 0WM W01M
ſ		Neither the	T	7
	True	one nor the	True	
		other		4
Pay is poor				Pay is good
]
				_
		Neither the		7
	True	one nor the	True	
There is plenty of		other		This job involves
variety in this			ł	doing the same task
· job			<u> </u>] all the time.
1				
l	True	Neither the	True	
	True	other	True]
Supervisors are				Supervisors are very
very helpful about				unhelpful about
work problems				problems
ī		Neither the	1	ר
	True	one nor the	True	
		other		
There is no free-				There is freedom to
dom to organise your own day's				organise your own day's work
work				1

4)	Given the tasks for the day, would you prefer?
	to have the day's work organised for you to organise your own work don't mind whether you organise the work or not.
5)	In practise, who does organise the day's work, or is the workmachine paced?

6)	How much information do you generally receive about your performance when work has been good?
	Too much About right Too little b) Is the way this is usually presented to you?
	Very acceptable Moderately acceptable Unacceptable
7)	How much information do you generally receive about your performance when work has been bad?
	Too much About right Too little

	b) Is the way this is presented to you?						
	Very acceptable						
	Modera	tely acce	eptable				
	Unacce	ptable					
	<u> </u>	-					
8)	Do any of the following	cause yo	ou difficulties	s in your job?			
		Rarely	Quite often	Most of the time			
	Heat						
	Walter	Rarely	Quite often	Most of the time			
	Noise						
		Rarely	Quite often	Most of the time			
	Fumes						
		Rarely	Quite often	Most of the time			
	Dust						
		<u> </u>	1				
		Rarely	Quite often	Most of the time			
	Vibration						
			L	L			
		Rarely	Quite often	Most of the time			
	Cold						
			<u> </u>	<u> </u>			

Draughts	Rarely	Quite often	Most of the time
Di auguvs			
	Rarely	Quite often	Most of the time
Cramped Conditions			
,			
	Rarely	Quite often	Most of the time
Poor Lighting			
b) If you answered "qui	te often"	to any of the	above, please sa
when the problem occ	urs.		
••••••	• • • • • • • •	•••••	• • • • • • • • • • • • • • • • • • • •
••••••	• • • • • • • •	•••••	• • • • • • • • • • • • • • • • • • • •
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c) Are any of the above	particul	arly troubleso	ne?
	• • • • • • • •	• • • • • • • • • • • • • • • • • • • •	• • • • • • • • • • • • • • • • •
	• • • • • • •	••••••	• • • • • • • • • • • • • • • • • • • •
•••••••	• • • • • • •	•••••	• • • • • • • • • • • • • • • •

9) While working do you wear amy of the following?

	Rarely	Quite often	Most of the time
Safety Helmets			
	Rarely	Quite often	Most of the time
Hearing Protection			
	Rarely	Quite often	Most of the time
Safety Glasses			
	Rarely	Quite often	Most of the time
Tinted Goggles			
	Rarely	Quite often	Most of the time
Gloves			
	Rarely	Quite often	Most of the time
Gauntlets			
			
	Rarely	Quite often	Most of the time
Sleeves			

Rarely

To all the	Rarely	Quite often	Most of the time	
Jacket				
	Rarely	Quite often	Most of the time	
Leggins				
	Rarely	Quite often	Most of the time	
Spats			·	
	Rarely	Quite often	Most of the time	
Safety Boots				
	Rarely	Quite often	Most of the time	
Other (Please say what)				
			_	
b) Are there any sit				
above items ought	to be worn	, but you don	't because	they are a
nuisance and get	in the way?	Please say w	hen :	
• • • • • • • • • • • • • • • • • • • •	• • • • • • • • •	• • • • • • • • • • • • • • • • • • • •	• • • • • • • • •	• • • • • • • • • •
• • • • • • • • • • • • • •			• • • • • • • • •	• • • • • • • • •
	• • • • • • • • • •	• • • • • • • • • • • • •	• • • • • • • • •	• • • • • • • • •
• • • • • • • • • • • • • • • • •	• • • • • • • • • •		• • • • • • • • • •	• • • • • • • • •
• 2 • • • 3 • • • • • • • • • •	• • • • • • • • • •	• • • • • • • • • • • • •	••••••	• • • • • • • • •

Most of the time

Quite often

Apron

10) Please indicate below your opinions of the standard of protective clothing made available for use in your job.

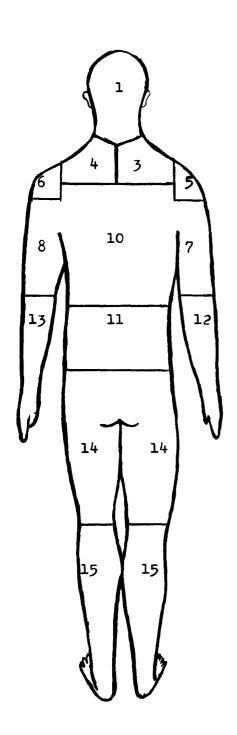
	Very good	Adequate	In need of improvement
Safety Helmet			
	Very good	Adequate	In need of improvement
Hearing Protection	G		
	Very	Adequate	In need of
Cafaty Classes	good	Aucquato	improvement
Safety Glasses			
	Very good	Adequate	In need of improvement
Tinted Goggles			
	Very goed	Adequate	In need of improvement
Gloves	good		Improvement
	Very		In need of
	good	Adequate	improvement
Gauntlets			
'			
	Very good	Adequate	In need of improvement
Sleeves	8-3-2		

	Very good	Adequate	In need of improvement		
Apron					
Jacket	Very good	Adequate	In need of improvement		
	Very good	Adequate	In need of improvement		
Leggins					
	Very good	Adequate	In need of improvement		
Spats					
G. C. A. D. L.	Very good	Adequate	In need of improvement	•	
Safety Boots					
	Very good	Adequate	In need of improvement		
Other (Please specify)					
b) If you answered "in need of improvement", please say what you feel is wrong with that particular item.					
	• • • • • • •	• • • • • • • • • • • •			
• • • • • • • • • • • • • • • • • • • •	• • • • • • • • •	• • • • • • • • • • • • • • • • • • • •	• • • • • • • • • • • • • • • • • • • •	• • • • • • • • • •	

Any other comments that you would like to make about the topics just considered?

SUPPLEMENT 3

Date	Shift	Time
Subjective Assess	ment of Fatigue of Specific	Parts of the Body
	Head and Neck	
	Eyes	
	R. Inner Shoulder	
	L. Inner Shoulder	
	R. Outer Shoulder	
	L. Outer Shoulder	
	R. Upper Arm	
	L. Upper Arm	
	Chest	
	Upper Back	
	Lower Back	
	R. Lower Arm and Hand	
	L. Lower Arm and Hand	
	Upper Legs	
	Lower Legs and Feet	



- 1. Head and Neck
- 2. Eyes
- 3. Right Inner Shoulder
- 4. Left Inner Schoulder
- 5. Right Outer Shoulder
- 6. Left Outer Shoulder
- 7. Right Upper Arm
- 8. Left Upper Arm
- 9. Chest
- 10. Upper Back
- 11. Lower Back
- 12. Right Lower Arm and Hand
- 13. Left Lower Arm and Hand
- 14. Upper Legs
- 15. Lower Legs and Feet

From the 15 parts of the body choose the 3 that feel the most uncomfortable. From the remaining 12 parts choose the next 3 most uncomfortable. Continue until 3 remain.

Dat	:e	Shift	Time	• • • • • •
	ease answer the two follows that best expresses h	lowing questions by marki how you feel <u>NOW</u> .	ng the point on t	the
1)	How generally tired do	you feel?		
	Not at alltired		Absoluted exhausted	l y i
2)	How different do the mu compared to those in the	uscles in your right/left ne other arm/shoulder?	arm/shoulder fee	: 1,
	No different		Completel different	L y t
3)	_	think you could continue		

Dat	e	. Shift Ti	me
a c	l <u>NOW</u> in relateross at the posson at the p	through each of the following and try to tion to the two end words or groups of wor pint on the line that best expresses your aple, a cross at the midpoint of the line you were feeling neither Happy nor Fed up.	ds, then place present strength
Hap	ру		Fed up
	Please work	through the list as quickly as possible.	
1)	Energetic		_ Exhausted
2)	Calm		_ Irritable
3)	Cheerful		_ Depressed
4)	Attentive		_ Bored
5)	In the mood for work		Not in the mood for work
6)	Miserable		_ Light-hearted
7)	Lazy		_ Active
8)	Tense		_ Relaxed
9)	Shattered		_ Refreshed
10)	Нарру		_ Fed-up

11)	Wide-awake	Sleepy	
12)	Vigorous	Washed	out
13)	Serious	Carefre	10

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